

# **WEST Search History**

DATE: Wednesday, June 26, 2002

Set Name	Query	<b>Hit Count</b>	Set Name
side by side			result set
DB = USPT, JPAB, EPAB, DWPI, TDBD; PLUR = YES; OP = OR			
L5	L4 and liposome\$	23	L5
L4	(carbonate) adj5 (glycerol)	541	L4
L3	(carbonate) adj10 (glycerol)	773	L3
L2	(carbonate) adj10 (distearoyl adj1 glycerol)	0	L2
L1	(carbonate) adj5 (distearoyl adj1 glycerol)	0	L1

END OF SEARCH HISTORY



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L5: Entry 8 of 23

File: USPT

Apr 18, 2000

DOCUMENT-IDENTIFIER: US 6051576 A

TITLE: Means to achieve sustained release of synergistic drugs by conjugation

Detailed Description Paragraph Right (26):

The codrug of the invention may be administered in injectable form selected from the group consisting of <a href="liposomes">liposomes</a>, liquids, suspensions and microsphere nanoparticles. Preparation of such aqueous solutions, <a href="liposomes">liposomes</a>, emulsion and suspensions are known to those of ordinary skill in the art (see Remington's Pharmaceutical Sciences, 18th Ed., Mack Publishing Co., Easton, Pa., 1990, pp. 1504-1712, incorporated herein by reference).

Detailed Description Paragraph Right (75):

The following is the structure of 5FU linked via a <u>carbonate bond to a glycerol</u> diflurbiprofen ester. The rationale is that the compound would hydrolyze in vivo to release 5FU, glycerol and two molecules of flurbiprofen.

#### CLAIMS:

4. A codrug according to claim 3, wherein said injectable form is selected from the group consisting of <a href="mailto:liposomes">liposomes</a>, suspensions, microsphere and nanoparticles.



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L3: Entry 11 of 58

File: USPT

Print

May 2, 2000

DOCUMENT-IDENTIFIER: US 6056973 A

TITLE: Therapeutic liposome composition and method of preparation

#### Drawing Description Paragraph Right (4):

FIG. 4 is a plot showing the blood circulation lifetime of target-cell sensitized <a href="liposome">liposome</a> prepared in accordance with the invention, where the percent of injected dose in vivo for <a href="liposome">liposome</a> having E-selectin Fab fragments targeting ligands (30 ligands per <a href="liposome">liposome</a> represented by solid triangles, 70 ligands per <a href="liposome">liposome</a> represented by solid squares) and for <a href="liposomes">liposome</a> having a surface coating of polyethyleneglycol chains (open circles) as a function of time after dosing; and

# Drawing Description Paragraph Right (5):

FIGS. 5A-5B are scanned images of micrographs of blood vessels in a window chamber of a mouse dorsal fold, where FIG. 5A is the control of the untreated blood vessels under transmitted light, and FIG. 5B is a fluorescence micrograph showing binding of fluorsecin-labeled <u>liposomes</u> bearing an E-selectin Fab fragments to endothelial cells in the blood vessels.

## Detailed Description Paragraph Right (66):

In studies performed in support of the invention, a targeting conjugate of the ligand sialyl-Lewis.sup.x was attached to PEG-DSPE according to known methods (DeFrees, S. A., et al., J. Am. Chem. Soc., 118:6101-6104 (1996)). Sialyl-Lewis.sup.x can be used to target liposomes to cells expressing endothelial leukocyte adhesion molecule-1 (ELAM-1 or E-selectin) for delivery of a therapeutic agent to a site of inflammation. ELAM-1 is expressed on the surface of endothelial cells of blood vessels adjacent to sites of inflammation. ELAM-1 recognizes and binds the polysaccharide moiety sialyl-Lewis.sup.x which is present on surfaces of neutrophils, and recruits neutrophils to sites of inflammation.

## Detailed Description Paragraph Right (75):

<u>Liposomes</u> having an E-selectin Fab fragment targeting ligand were prepared in accordance with the invention for in vivo administration to rodents. As described in Example 2, an anti-E-selectin Fab fragment was conjugated to PEG-DSPE to form an E-selectin Fab-PEG-DSPE targeting conjugate. The targeting conjugate was incubated with pre-formed .sup.111 In-labelled-liposomes composed of partially hydrogenated soy phosphatidylcholine (PHPC), PEG-DSPE and cholesterol in a 55:40:3 molar ratio in an amount sufficient to obtain 12, 20, 33, 40 and 70 Fab residues per 100 nm liposome (Example 2B). The insertion procedure resulted in greater than 95% of the targeting conjugates being inserted into the pre-formed liposomes. In one embodiment of the invention, the insertion efficiency is greater than 90%, more preferably greater than 95%.

# Detailed Description Paragraph Right (77):

As described in Example 2C, pre-formed <u>liposomes</u> composed of hydrogenated soy phosphatidylcholine (HSPC), cholesterol, <u>PEG-DSPE</u> and fluorescein-labelled DHPE, in a molar ratio of 53.5/40/4/2.5, were incubated with the <u>E-selectin-PEG-DSPE</u> targeting conjugate at 37.degree. C. for 1 hour. The fluorescein-labeled <u>liposomes</u> were administered to mice equipped with a dorsal skin fold window chamber. Endotoxin was applied topically in the window chamber 10 minutes after intravenous injection of the <u>liposomes</u>. FIGS. 5A-5B are scanned images of photomicrographs of the blood vessels under transmitted light prior to <u>liposome</u> administration (FIG. 5A) and 5 hours after administration of the target-cell sensitized, fluorescein-labeled liposomes (FIG.



Detailed Description Paragraph Right (78):

As can be seen in FIG. 5B, the E-selectin Fab liposomes target the endothelial cells along the blood vessels. The appearance of E-selectin antigen peak was around 5 hours after endotoxin treatment, indicating that the binding activity of the E-selectin antibody was retained.

Detailed Description Paragraph Right (119):

E-selectin Fab-PEG-DSPE targeting conjugate was inserted into pre-formed liposomes as follows. The pre-formed  $\underline{\text{liposomes}}$  were composed of hydrogenated soy phosphatidylcholine (HSPC), cholesterol and PEG-DSPE in a molar ratio of 53.5/40/4. The <u>liposomes</u> included 2.5 mole percent of the lipid marker of fluorescein-DHPE (Molecular Probes, Inc.). The pre-formed liposomes were incubated with the micellular solution of the targeting conjugate at 37.degree. C. for 1 hour. The insertion mixture was placed on a Bio-Rad A50m column equilibrated with 25 mM HEPES/saline pH 7.2 and 0.5 ml fractions were collected. Spectrophotometric analysis of the fractions indicated that the insertion efficiency of the Fab targeting conjugate into the liposomes was approximately 100% after 2 hours at 37.degree. C.

Detailed Description Paragraph Center (6):

Preparation of Anti-E-selectin Fab Conjugate and Insertion into Pre-formed Liposomes